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- 3 1. Apparatus for the measurement of vascular
- 4 impedance of the ocular micro circulation in vivo,
- 5 comprising intra-ocular pressure measurement means
- 6 from which a pressure pulse waveform is calculable,
- 7 blood velocity profile measurement means for
- 8 measuring the linear blood flow velocity in the
- 9 retrobulbar circulation, and means for calculating a
- 10 vascular impedance modulus from the pressure pulse
- 11 waveform and the linear blood flow velocity.

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- 13 2. Apparatus as claimed in claim 1, wherein the
- 14 intra-ocular pressure measurement means is suitable
- 15 for measuring the maximum and minimum pressure
- 16 values of the pulse profile to calculate a mean
- 17 intra-ocular pressure.

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- 19 3. Apparatus as claimed in claim 1 or claim 2,
- 20 suitable for measuring how the pressure pulse
- 21 waveform and the linear blood flow velocity vary
- 22 over the period of a respiratory cycle.

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- 24 4. Apparatus as claimed in any preceding claim,
- 25 wherein a solid state transducer is used to measure
- 26 intra-ocular pressure.

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- 28 5. Apparatus as claimed in claim 4, wherein a
- 29 suitable solid state transducer operates in
- 30 conjunction with a suitable telemetry system to
- 31 process the data.

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- Apparatus as claimed in any of claims 1 to 3, 1
- wherein an ocular pneumotonometer is used to measure 2
- intra-ocular pressure. 3

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- Apparatus as claimed in any preceding claim, 5 7.
- wherein the blood velocity profile measurement means 6
- is an ultrasound device. 7

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- Apparatus as claimed in claim 7, wherein the 9 8.
- ultrasound device is a doppler ultrasound imager. 10

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- Apparatus as claimed in any preceding claim 9. 12
- further comprising motion picture generation means 13
- to produce moving images of an artery. 14

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- Apparatus as claimed in claim 9, wherein the 16
- moving images are capable of being used to ensure 17
- that a user of the apparatus can accurately identify 18
- the location of an artery. 19

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- Apparatus as claimed in any preceding claim, 21
- wherein the change in the pulsatile intra-ocular 22
- pressure waveform and the linear blood flow velocity 23
- are measured sequentially. 24

- Apparatus as claimed in any preceding claim, 26
- wherein the means for calculating the vascular 27
- impedance modulus comprises means for; 28
- obtaining the fourier transform of the intra-29
- ocular pressure pulse waveform and the linear blood 30
- flow velocity and dividing the transformed values of 31
- the pulsatile change in the intra-ocular pressure 32

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- 1 pulse by the transformed retrobulbar blood flow
- 2 velocity.

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- 4 13. Apparatus as claimed in any preceding claim,
- 5 wherein the pulsatile change in intra-ocular
- 6 pressure has a phase associated therewith.

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- 8 14. Apparatus as claimed in any preceding claim,
- 9 wherein the intra-ocular blood velocity has a phase
- 10 associated therewith.

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- 12 15. A method for the measurement of vascular
- 13 impedance of the ocular micro circulation in vivo,
- 14 comprising the steps of: measuring the intra-ocular
- 15 pressure pulse waveform of the ocular network;
- 16 measuring the linear blood flow velocity in the
- 17 retrobulbar circulation; and
- 18 calculating the vascular impedance modulus from the
- 19 intra ocular pressure pulse waveform and the linear
- 20 blood flow velocity waveform.

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- 22 16. A method as claimed in claim 15, wherein the
- 23 pressure pulse waveform and the linear blood flow
- 24 velocity are measured over the period of a
- 25 respiratory cycle, and their variation therewith is
- 26 measured.

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- 28 17. A method as claimed in claim 16, wherein the
- 29 variations are used in the calculation of the
- 30 vascular impedance modulus.

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- 1 18. A method as claimed in any of claims 15 to 17,
- 2 further comprising the steps of recording moving
- 3 images of an artery.

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- 5 19. A method as claimed in claim 18, wherein the
- 6 moving images are used to accurately identify the
- 7 location of an artery.

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- 9 20. A method as claimed in any of claims 15 to 19,
- 10 wherein the change in the pulsatile intra-ocular
- 11 pressure waveform and the linear blood flow velocity
- 12 are measured sequentially.

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- 14 21. A method as claimed in any of claims 15 to 20,
- 15 wherein the step of calculating the vascular
- 16 impedance modulus comprises the steps of;
- 17 obtaining the fourier transform of the intra-ocular
- 18 pressure pulse waveform and the linear blood flow
- 19 velocity and dividing the transformed values of the
- 20 pulsatile change in the intra-ocular pressure pulse
- 21 by the transformed retrobulbar blood flow velocity.